



Stanford Cancer Imaging
Training Program

Technology development for a 100 picosecond coincidence time resolution time-of-flight positron emission tomography system

Shirin Pourashraf

(shirinp1@Stanford.edu)

Stanford Cancer Imaging Training (SCIT) Seminar / RSL Weekly Seminars

Mentored by: Drs. [Andrei Iagaru](#), M.D. & [Craig Levin](#), Ph.D.



MIPS

Molecular Imaging
Program at Stanford

Jan. 11th, 2023

Stanford University

School of Medicine
Department of Radiology



Positron Emission Tomography (PET) System



Stanford Cancer Imaging
Training Program

- **%80 of PET usage in Cancer:**
 - Detecting and staging specific types of cancer and/or assessing response to treatment
- **Cardovascular and/or Neurological Disease**
 - Evaluating the function of organs, such as the heart and/or brain



MIPS

Molecular Imaging
Program at Stanford

Stanford University

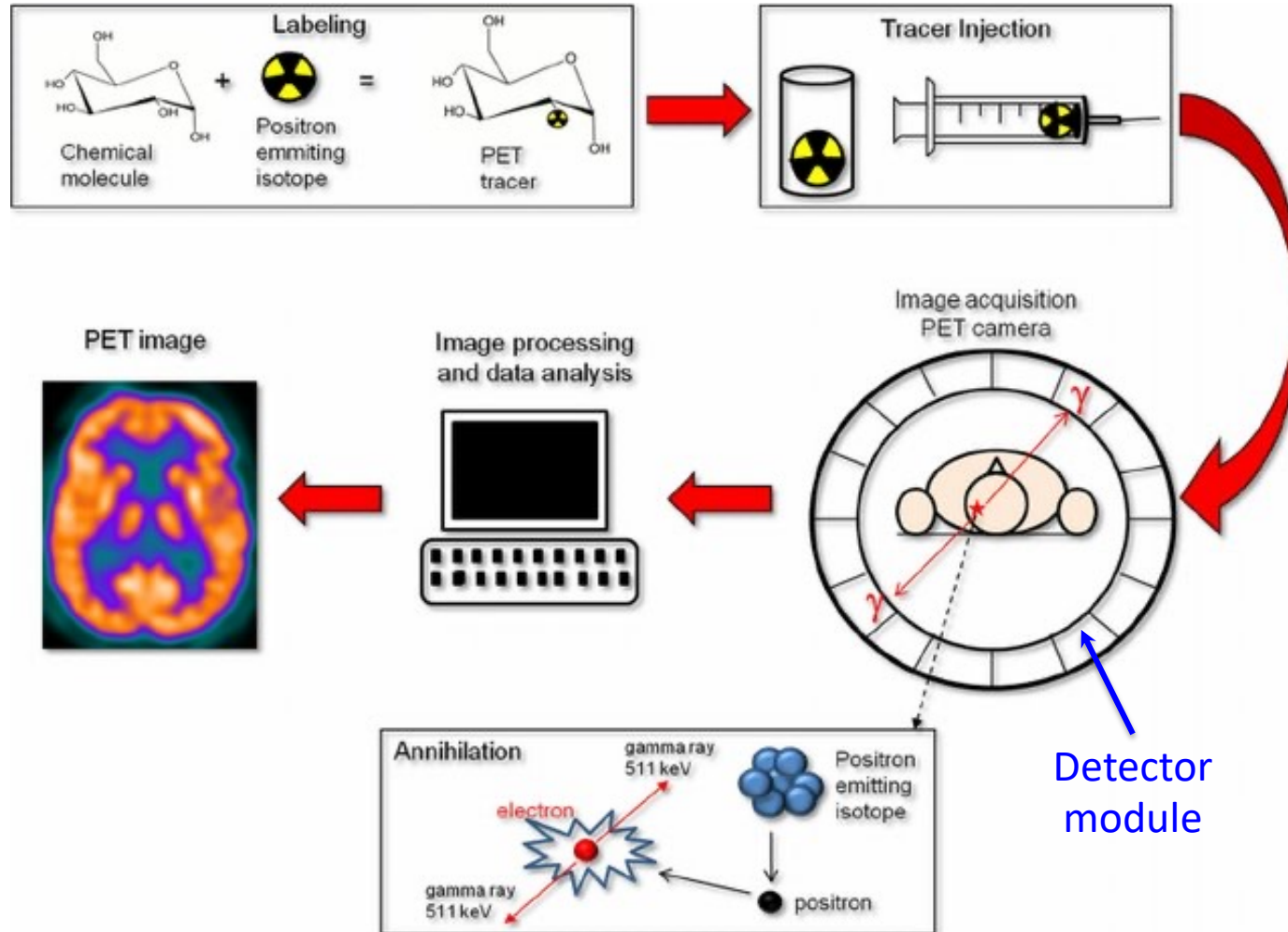
School of Medicine
Department of Radiology



Concept Behind PET



Stanford Cancer Imaging
Training Program



- Positron emitter radionuclides
 - e.g ^{11}C , ^{13}N , ^{15}O , & ^{18}F
- Ring of Detector modules
 - Scintillation crystals + photosensor + electronic readout
- Event localization along lines of response (LOR)
 - Arrival time difference of coincident events



MIPS

Molecular Imaging
Program at Stanford

Stanford University

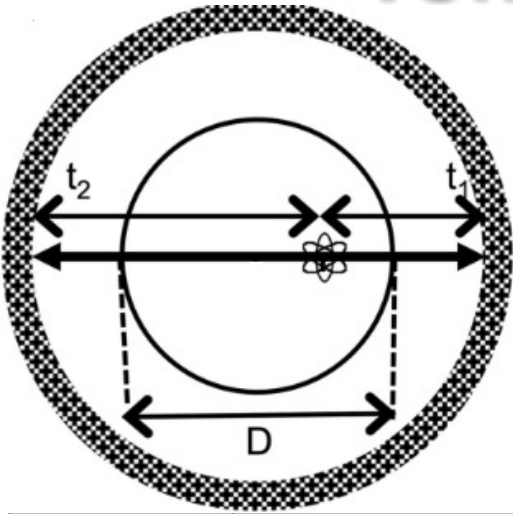
School of Medicine
Department of Radiology



Time of Flight Positron Emission Tomography (TOF-PET)

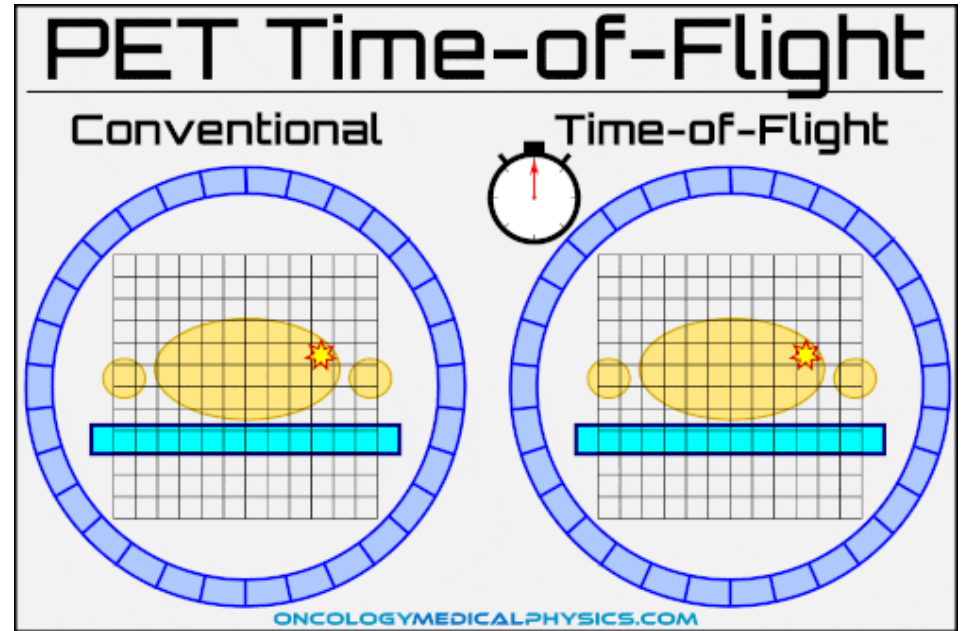


Stanford Cancer Imaging Training Program



- $\Delta t = t_2 - t_1$: Arrival time difference between photons in coincident events
- **CTR (Coincidence Time Resolution)**: FWHM of Δt distribution
- **D**: Patient diameter (e.g. 40 cm)
- **c = 3×10^{10} cm/s**: speed of light
- **$\Delta x = c \times \text{CTR}/2$** : Localization error

<https://oncologymedicalphysics.com/nuclear-tomographic-imaging/>



$\Delta x > D$

Equal probability in all voxels along the LOR ☹️

$\Delta x < D$

Confined probability to a small segment on the LOR ☺️

CTR (ps)	$\Delta x = c \times \frac{\text{CTR}}{2}$	Gain = $\frac{SNR_{TOF}}{SNR_{Non-TOF}} \approx \sqrt{\frac{D}{c \times \frac{\text{CTR}}{2}}}$
1000	15 cm	1.6
500	7.5 cm	3.1
400	6 cm	2.6
214	3.7 cm	3.5
100	1.5 cm	5.2



MIPS

Molecular Imaging Program at Stanford

Stanford University

School of Medicine
Department of Radiology



State-of-the-Art: 214 ps CTR TOF-PET/CT

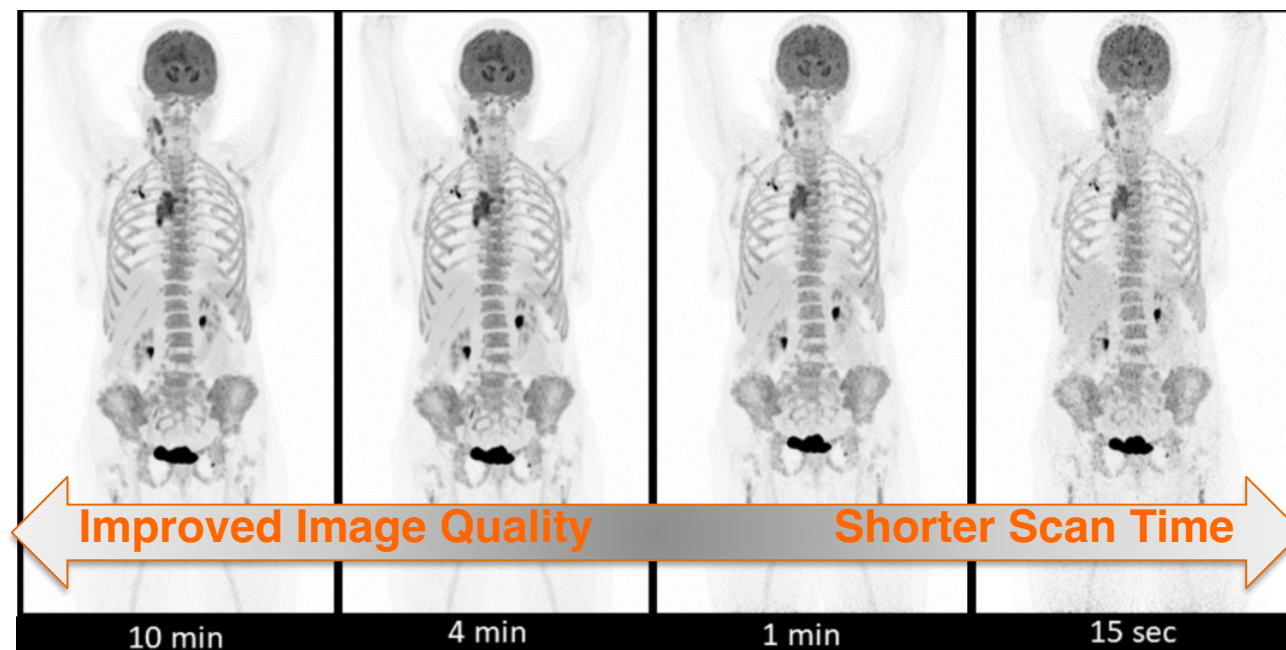


Stanford Cancer Imaging
Training Program

<https://www.siemens-healthineers.com/en-us/molecular-imaging/pet-ct/biograph-vision-quadra>



Single Bed Position Images



- **Improved CTR (214 ps) and localization along LOR (3.7 cm)**
 - Improved reconstructed image SNR, signal-to-background ratio, image quality, accuracy, and lesion detectability
- **or getting the same image quality as Conventional PET**
 - Lower injected dose to patients or shorter scan time
 - Wider category of patients can be served



MIPS
Molecular Imaging
Program at Stanford

Stanford University

School of Medicine
Department of Radiology



System Level Electronic Readout for TOF-PET



Stanford Cancer Imaging
Training Program

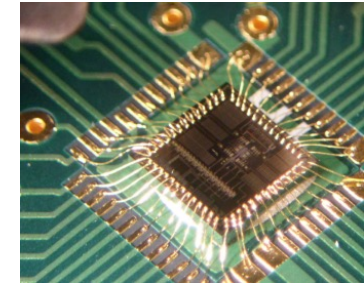
- At system level, 214 ps is the best commercially-available CTR (Biograph TOF-PET/CT)
- Currently several benchtop experiments with CTR ≤ 100 ps using single-pixel detectors
 - Challenging to scale results up to full system

System Design Approaches:

- One-to-one coupling of scintillation crystals to compact sized SiPMs:
 - × Large number of electronic readout channels needed
 - × Costly, not power efficient, and heat generated degrading SiPM performance, especially CTR

- Designing ASICs

- × Long design time
- × Also costly



Multiplexing:

- Simply hardwiring SiPMs signals together
 - × Parasitic capacitance $\gg \gg$ CTR degradation
- Resistive charge division
 - × High RC constant $\gg \gg$ CTR degradation
- Delay-line method
 - × Lower SNR, especially for longer delays
 - × Requiring more resources from FPGA



MIPS

Molecular Imaging
Program at Stanford

Stanford University

School of Medicine
Department of Radiology

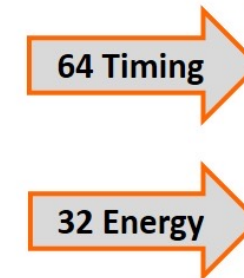
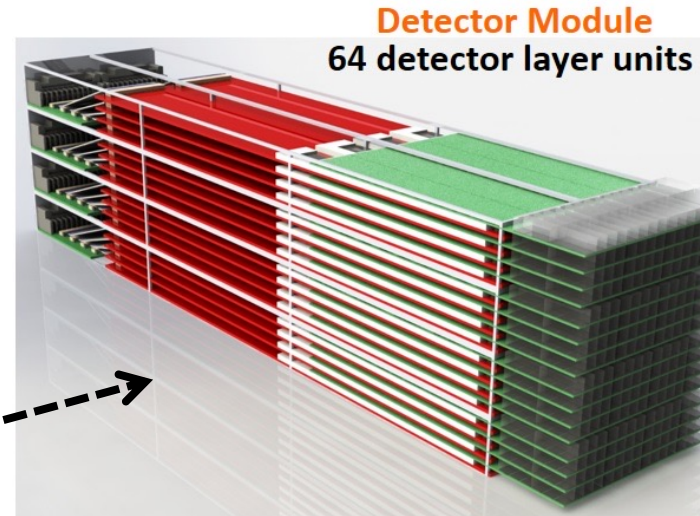
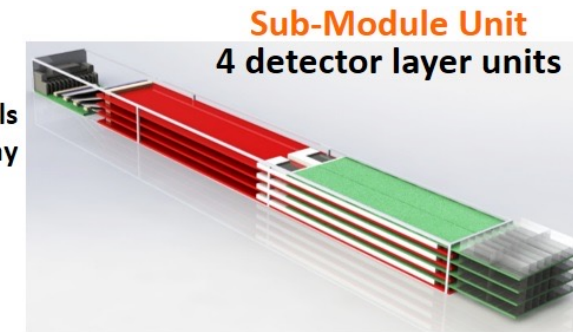
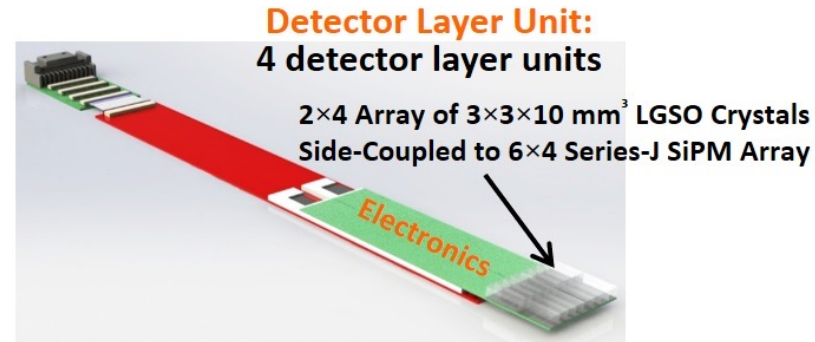
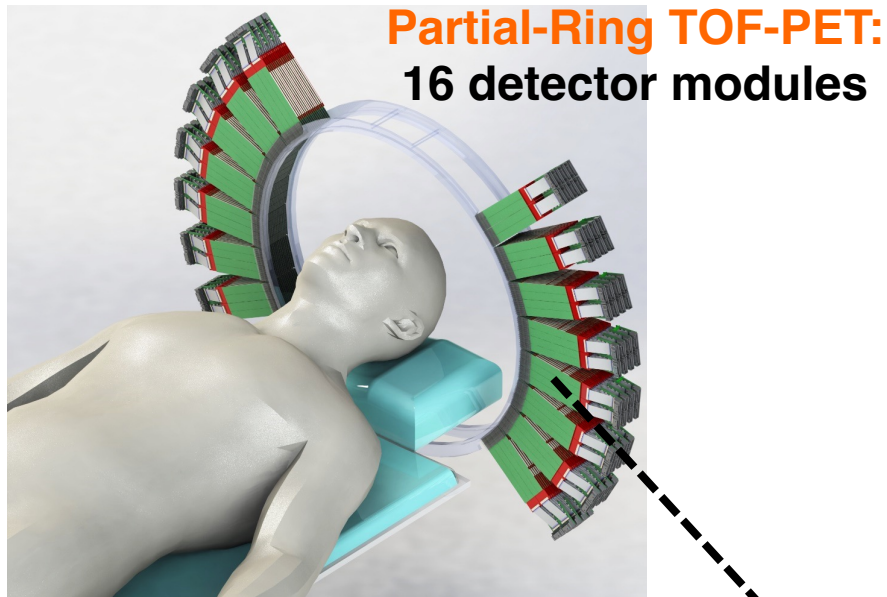


Scale-Up Scheme of 100 ps TOF-PET



Stanford Cancer Imaging Training Program

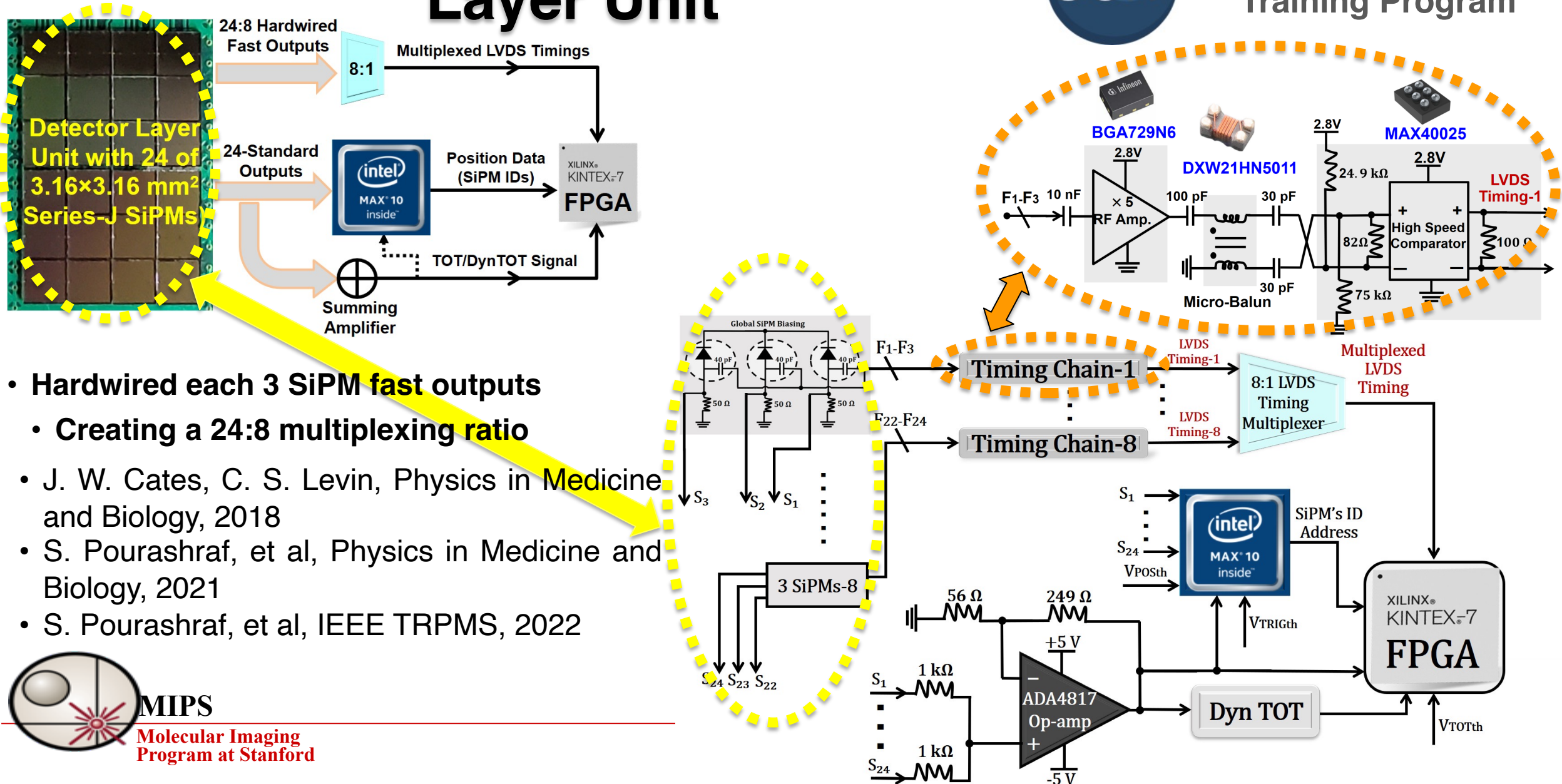
- J. W. Cates, C. S. Levin, Physics in Medicine and Biology, 2018
- S. Pourashraf, et al, Physics in Medicine and Biology, 2021
- S. Pourashraf, et al, IEEE TRPMS, 2022



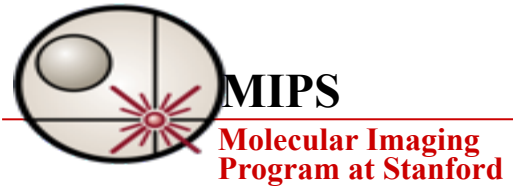
Electronic Read-out of Detector Layer Unit



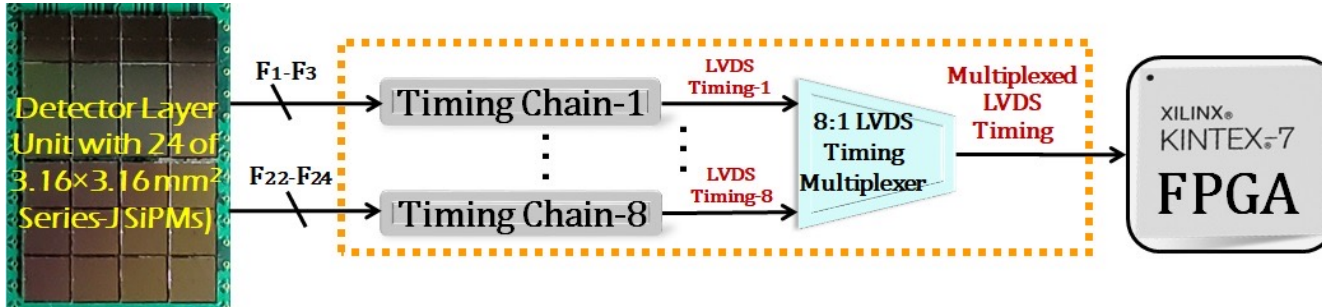
Stanford Cancer Imaging Training Program



- **Hardwired each 3 SiPM fast outputs**
- **Creating a 24:8 multiplexing ratio**
- J. W. Cates, C. S. Levin, Physics in Medicine and Biology, 2018
- S. Pourashraf, et al, Physics in Medicine and Biology, 2021
- S. Pourashraf, et al, IEEE TRPMS, 2022



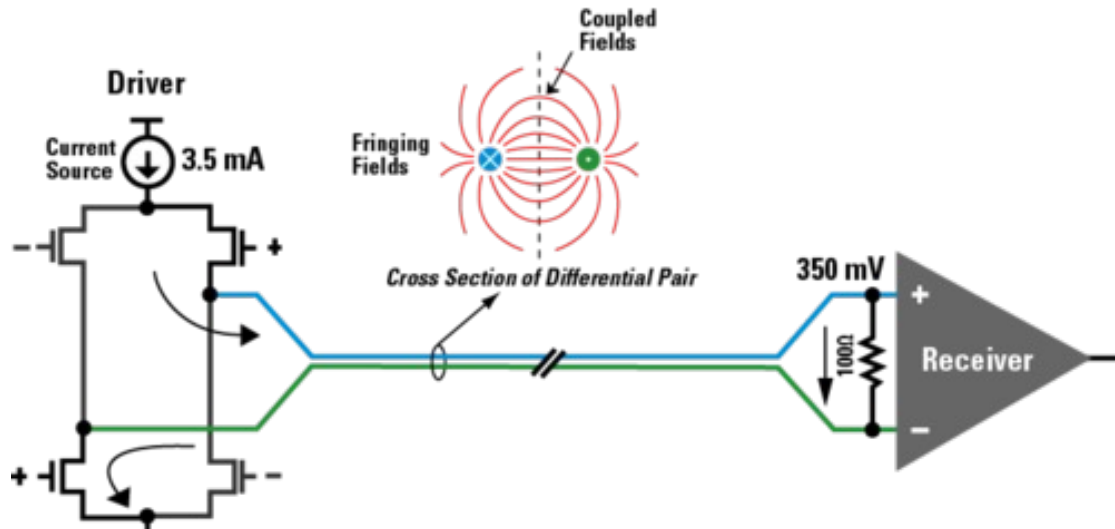
Multiplexing of Timing Channels



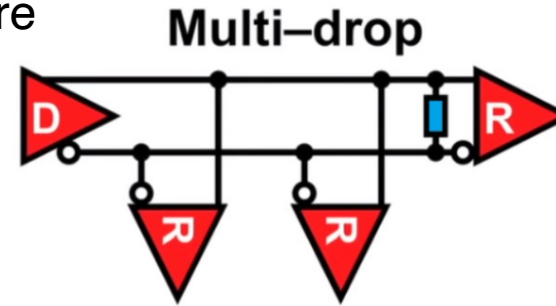
- **Not aware of an electronic component to efficiently combine our sharp edge LVDS timings!**

Why not simply combine LVDS signals?

- Standard LVDS has several advantages, but are current mode drivers not voltage!



<https://www.ti.com/lit/an/snla375/snla375.pdf?ts=1667664571867>

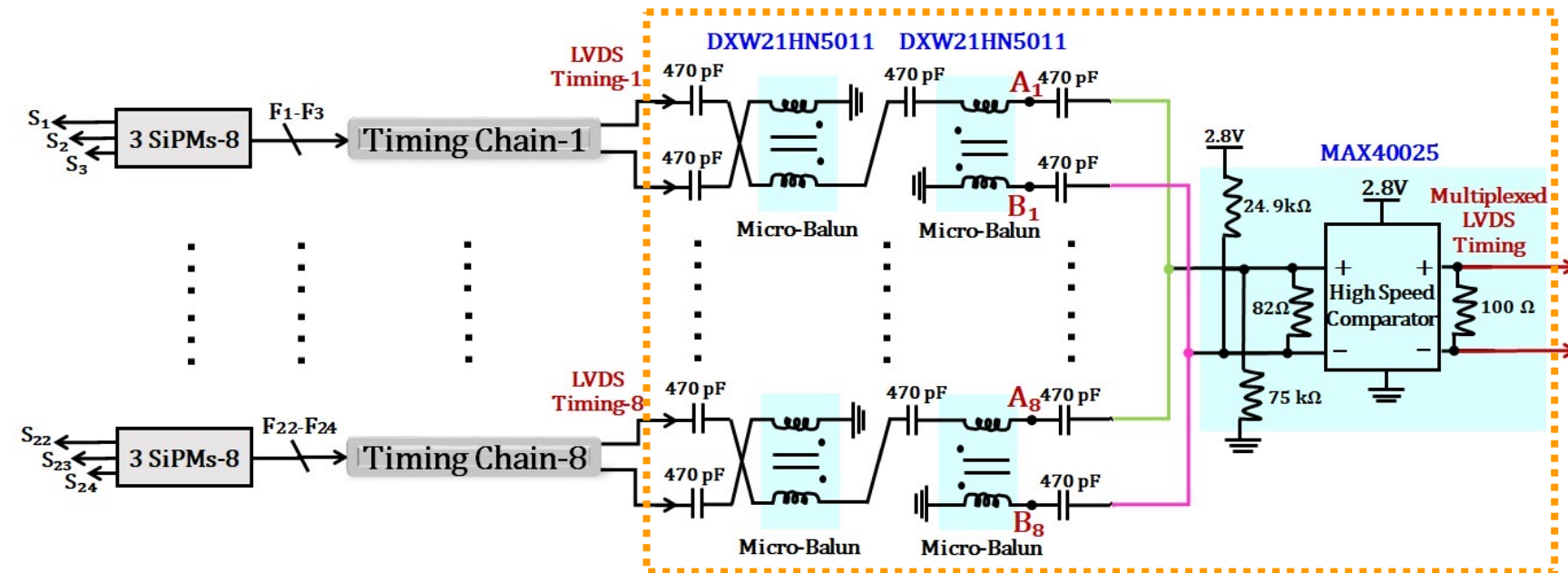


- But our case, several drivers (D) hanging off a main bus line with one receiver (R) at the end!

- Impedance mismatch and reflection due to stubs (unterminated length of drivers to the main bus)
- Needs careful considerations
 - Otherwise signal integrity issue, increased jitter, and loss of information



Our 24:1 Timing Multiplexing Approach



- Only passive micro-baluns and one extra comparator used
 - Saving footprint
 - Cost effective
 - Power efficient
- Just 4.5 mW/Channel extra power dissipation!**

• Converting 8-LVDS timing signals to single-ended outputs using passive micro-baluns

• Then again converting these single-ended outputs to differential signals using micro-baluns

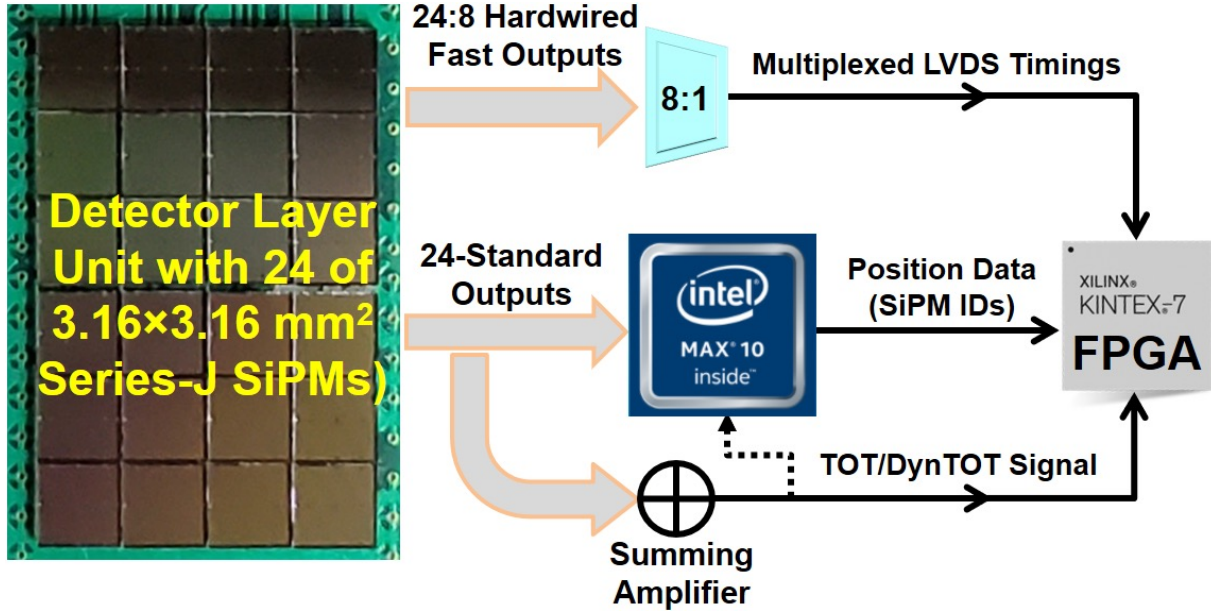
• Finally, hardwiring these 8 differential timing outputs at nodes $A_{1...8}$ & $B_{1...8}$ inputting the differential pins of the last MAX40025 comparator to produce the final LVDS timing channel



PCBs for System Development

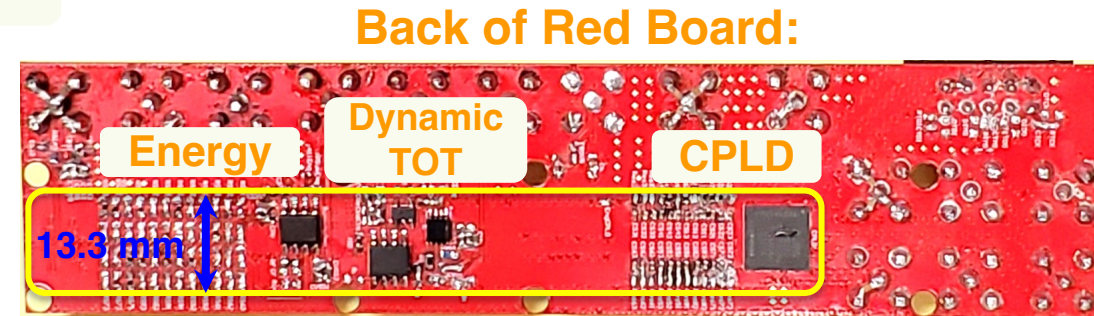
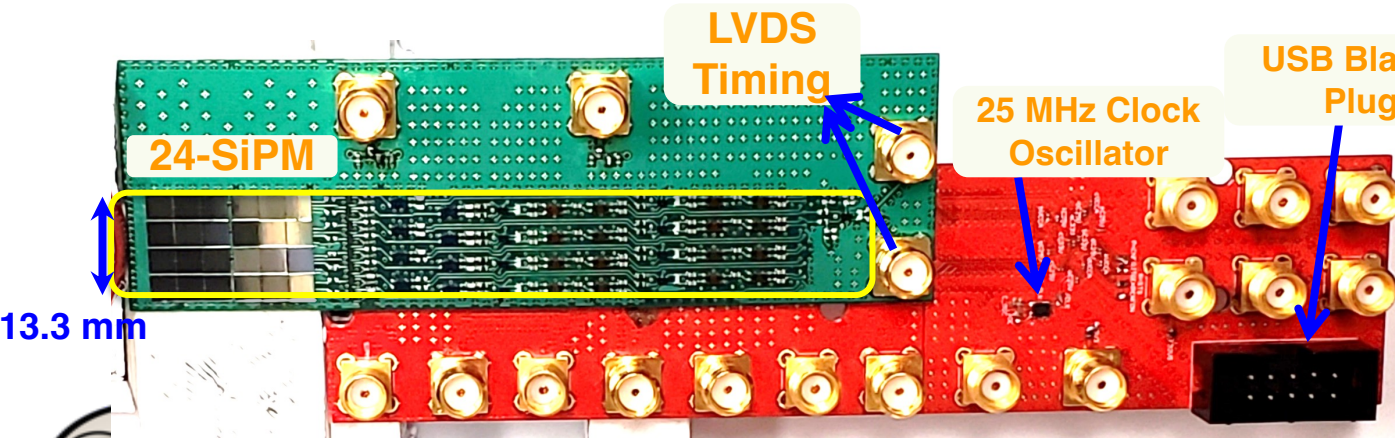


Stanford Cancer Imaging Training Program



- **Compact and scalable**

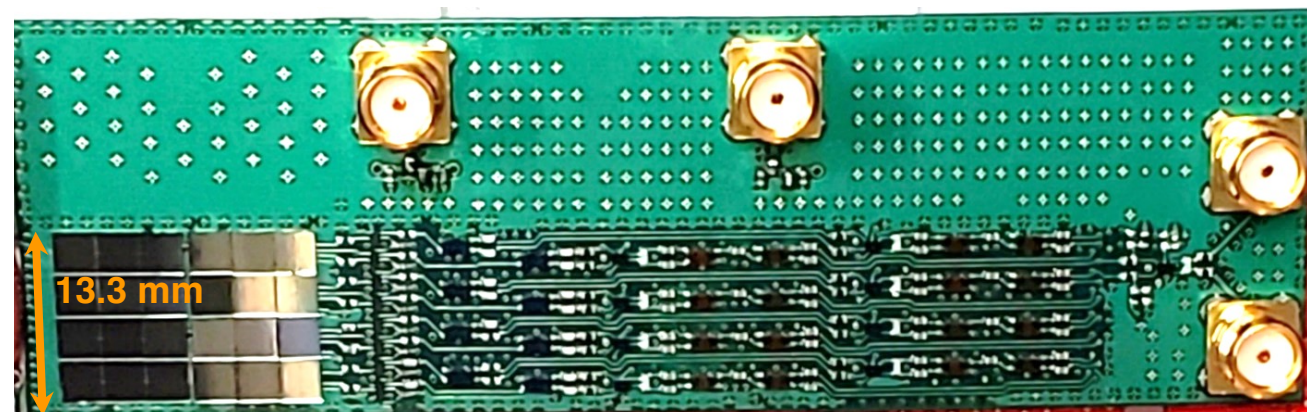
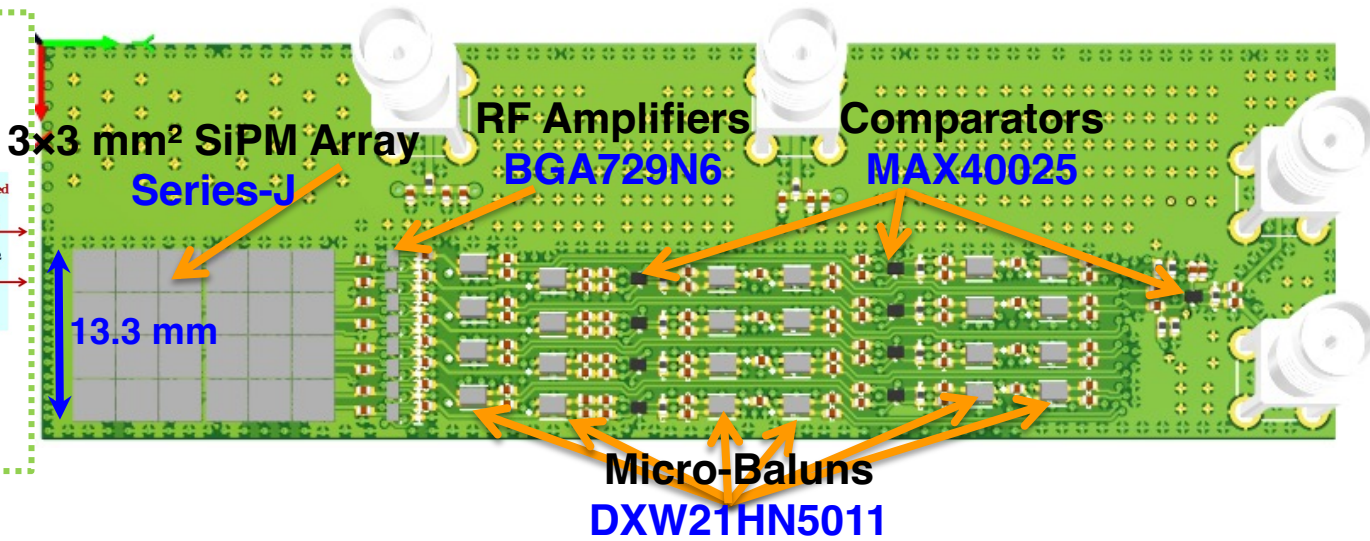
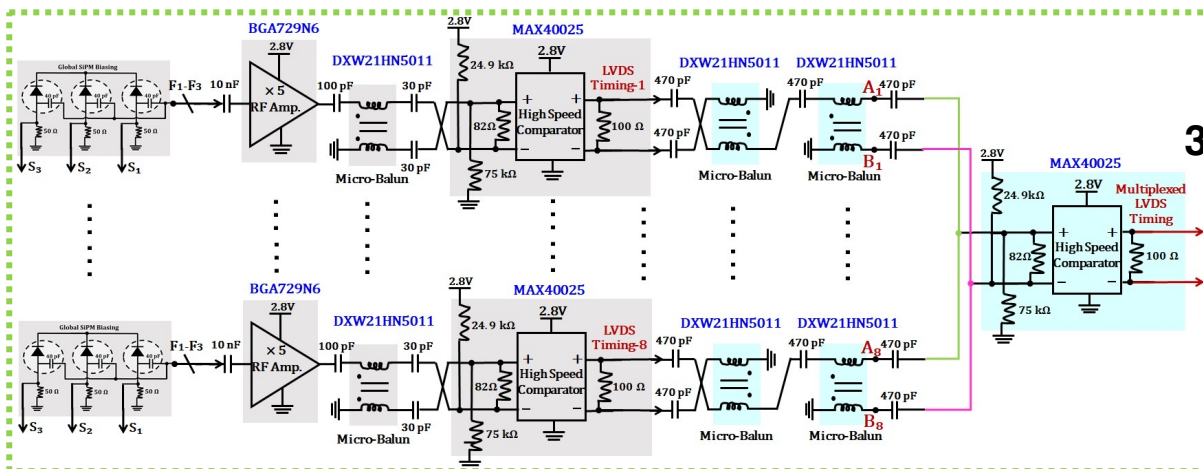
- Timing chain implemented in 13.3 mm width of a 4-layer FR4 PCB (green board)
- 4x6 array of 3x3 mm² SiPMs on timing board
- Energy chain implemented in 13.3 mm width of a 6-layer FR4 PCB board (red board)



PCB and Physical Implementation



Stanford Cancer Imaging Training Program



- Multiplexing chain:
 - Didn't increase the 13.3 mm width of our PCB 😊
 - ✓ High sensitivity remains
 - Increased the length of PCB only ~27 mm
 - ✓ Should not have effect on increasing jitter as the timing signals are already digitized! 😊



MIPS
Molecular Imaging Program at Stanford

Stanford University

School of Medicine
Department of Radiology

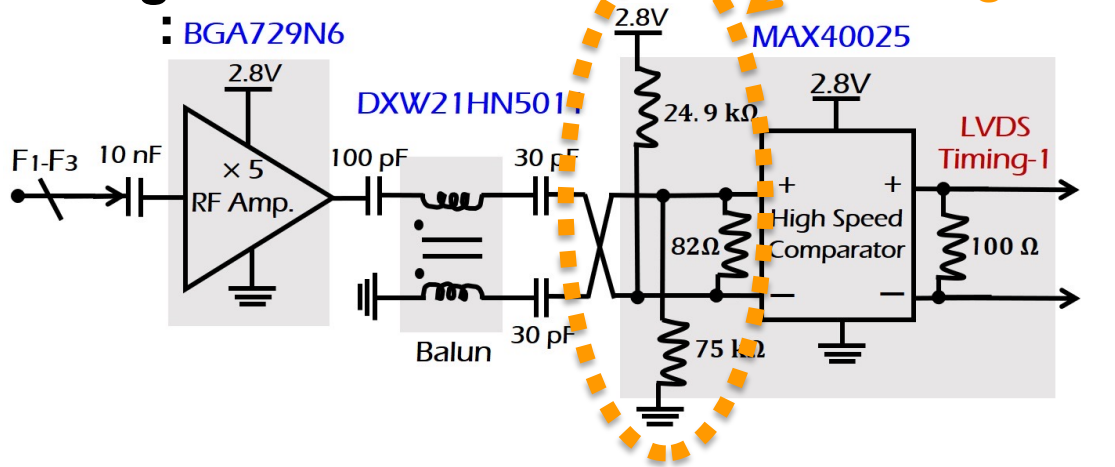


Fail-Safe Biasing for Comparators

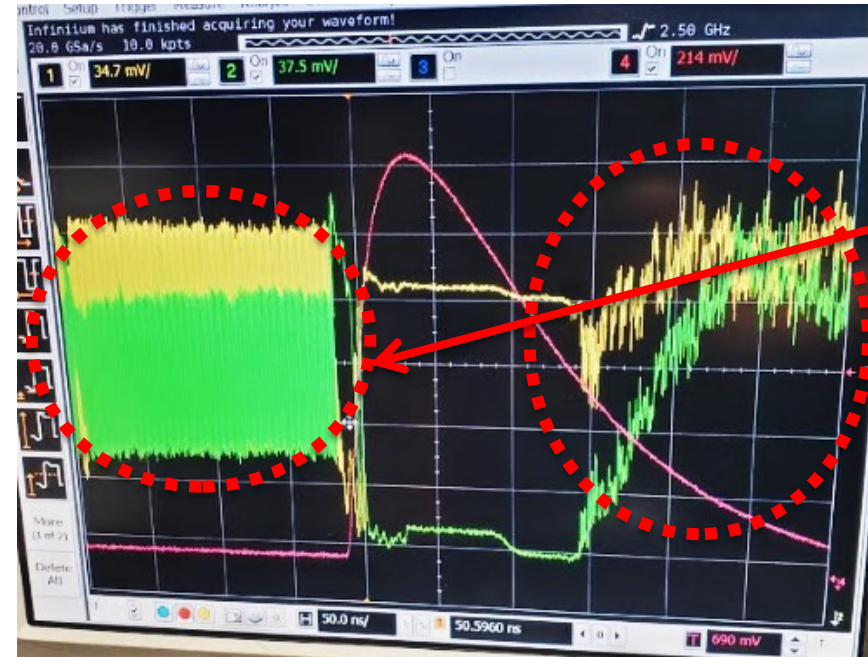


One channel Timing Chain

• BGA729N6



- External fail-safe resistive biasing at the differential inputs of all MAX40025 comparators
 - It provided 2.1 V common mode voltages for comparator's positive and negative inputs
 - It also provided $V_{id} = -2.5 \text{ mV}$ dropped on 82 Ω line termination resistors of comparator to clean up the LVDS timing signals at **idle line states**



Idle line state problem

- Careful selection of resistive network is needed as it can introduce more jitter
- In our system, V_{id} can be $< 2.5 \text{ mV}$ as the noise level is very low ($\sim 1 \text{ mV}$)



MIPS

Molecular Imaging Program at Stanford

Stanford University

School of Medicine
Department of Radiology

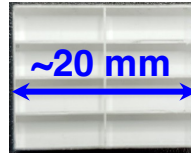


Experiments with 24:1 Timing Multiplexing Readout

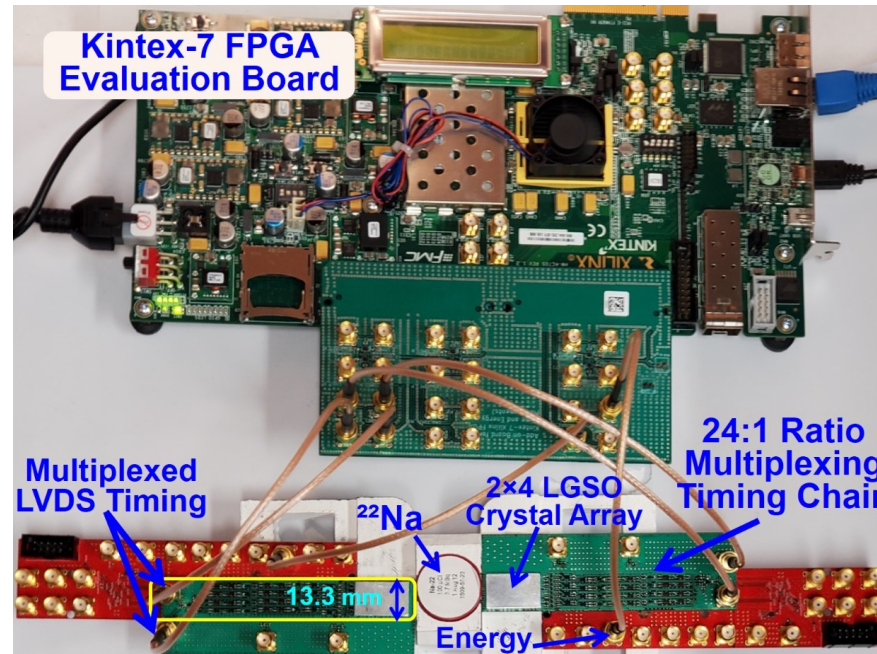
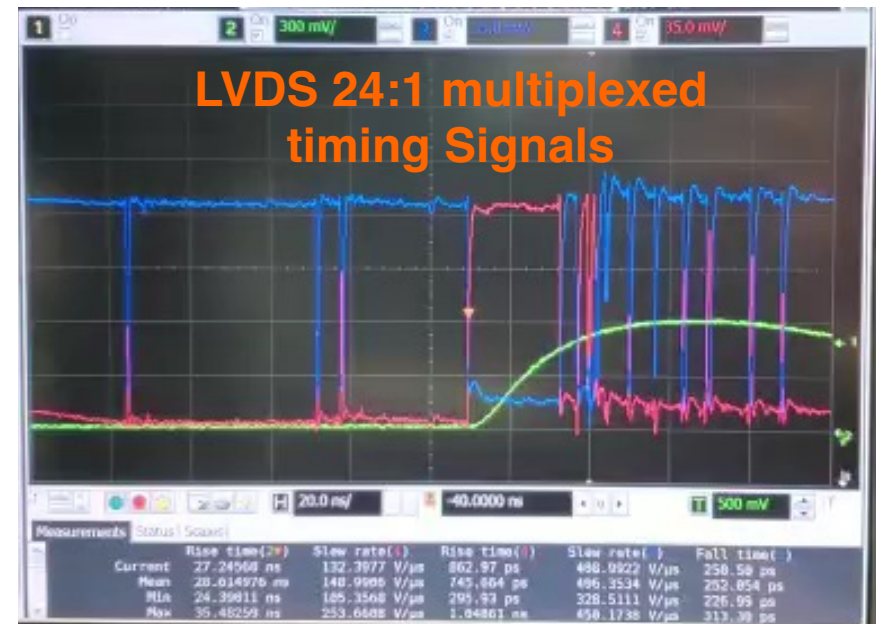


Stanford Cancer Imaging Training Program

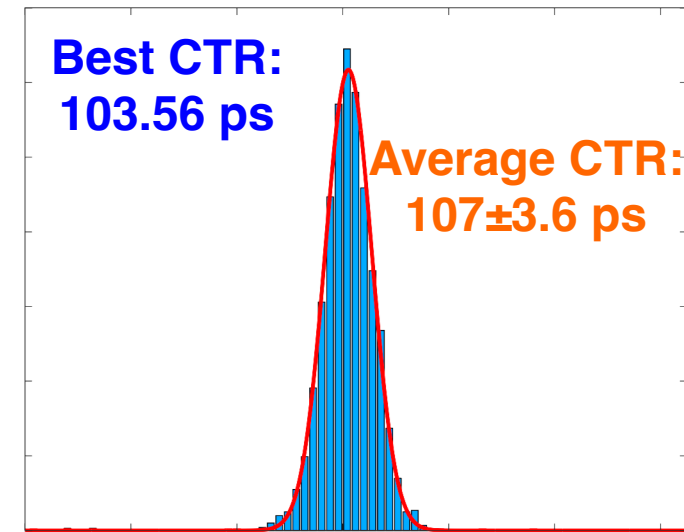
- LVDS 24:1 multiplexed timing signals of one detector unit (**Positive & Negative**)
 - Using 2x4 array of 3x3x10 mm³ fast LGSO crystal coated with BaSO₄ reflector
 - Triggered with **Energy Signal**



- Combined 24 SiPMs' fast output
 - 24:1 SiPM-to-channel multiplexing
- Average CTR of **107±3.6 ps** over multiple measurements @ optimum 31 V SiPM biasing
 - Near to 100 ps CTR as single 10 mm crystal detector 😊



CTR of 24:1 Multiplexed Timing



MIPS
Molecular Imaging Program at Stanford

Stanford University

School of Medicine
Department of Radiology



Some Other Time of Flight Applications



Stanford Cancer Imaging
Training Program

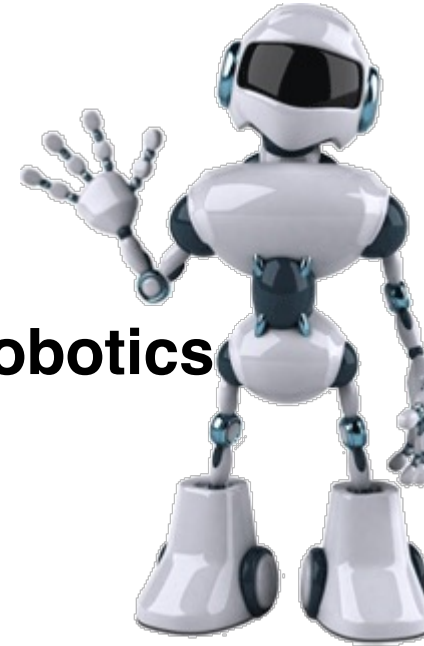
Light Detection And Ranging



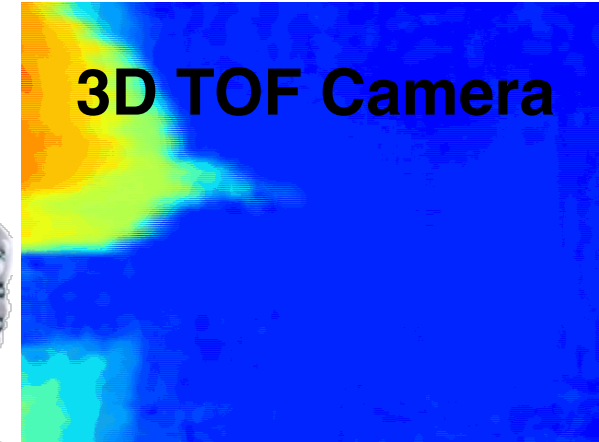
Automotive



Robotics



3D TOF Camera



- This 24:1 timing multiplexing method also has the potential to be used in other TOF applications due to:
 - Simplicity and Scalability
 - Cost/Area/Power Efficiency
 - **Most importantly, its “Ease of Implementation” & “Robustness”**



MIPS

Molecular Imaging
Program at Stanford

Stanford University

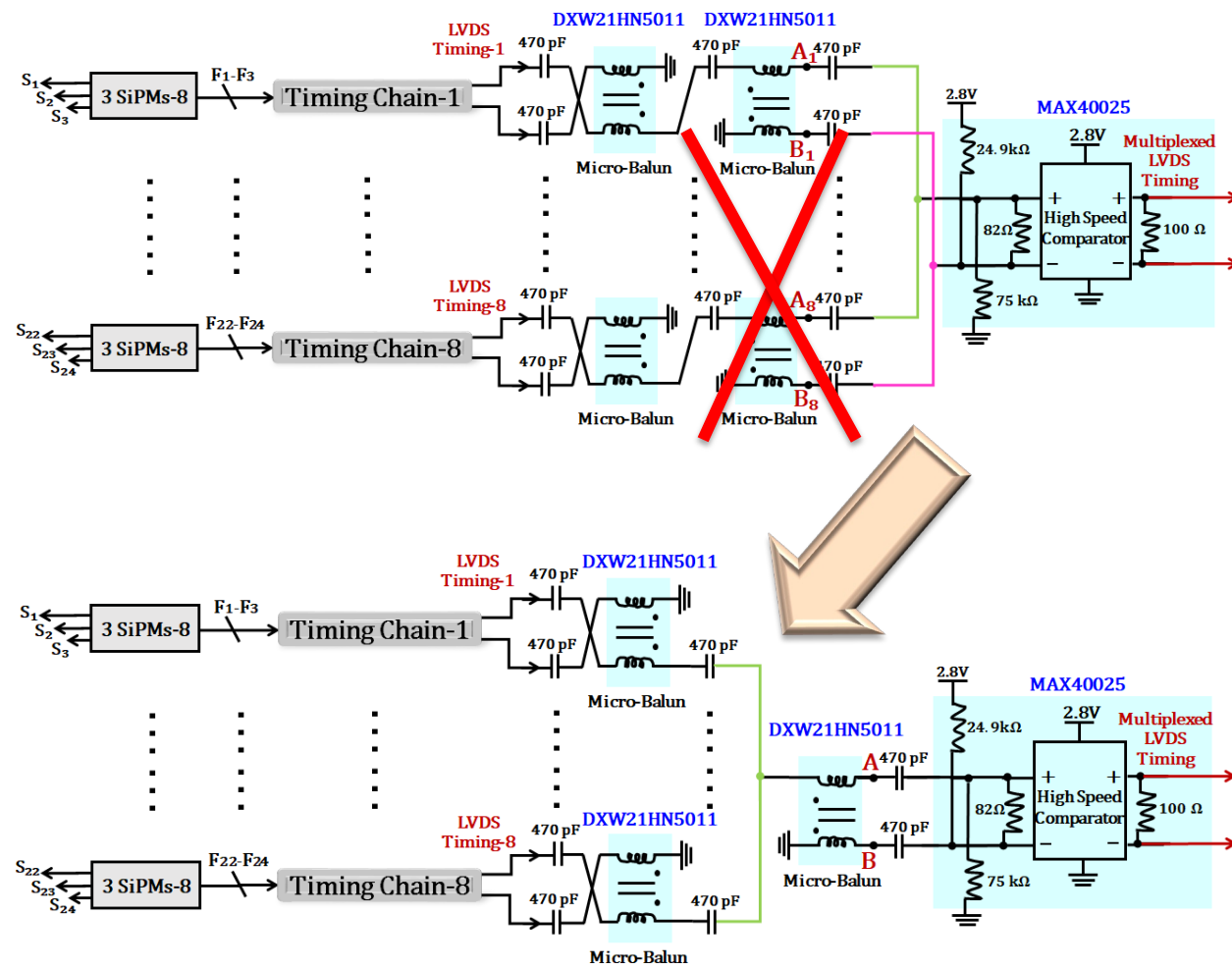
School of Medicine
Department of Radiology



Discussion

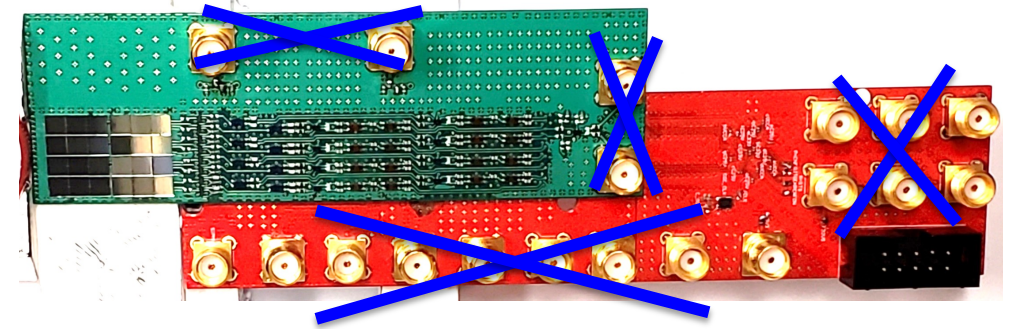


- **Effective implementation of compact TOF-PET detector layer**
 - Combined 8-timing channels (24 SiPM's fast outputs)
 - **107 ps FWHM CTR** for 20 mm long crystal elements
 - 1.1 W power dissipation per detector unit layer
- **Simpler possible version of the multiplexing scheme**
 - Should mostly perform the same
 - Saving 7 micro-baluns
- **There is a high potential this multiplexing scheme can serve more than 24 SiPMs (e.g. 48)**

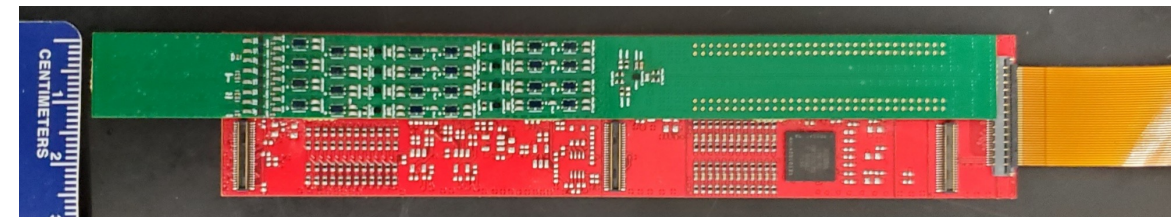


Next Steps:

Previous Readout with SMA Connectors



Under Test SMA-less Readout
(Challenging to test)



- Each two **timing boards** will be mounted on a **10-layer FR4 red board** assigned for energy and positioning assessment

- **Currently** testing SMA-less Detector Layer Units (highly compact)

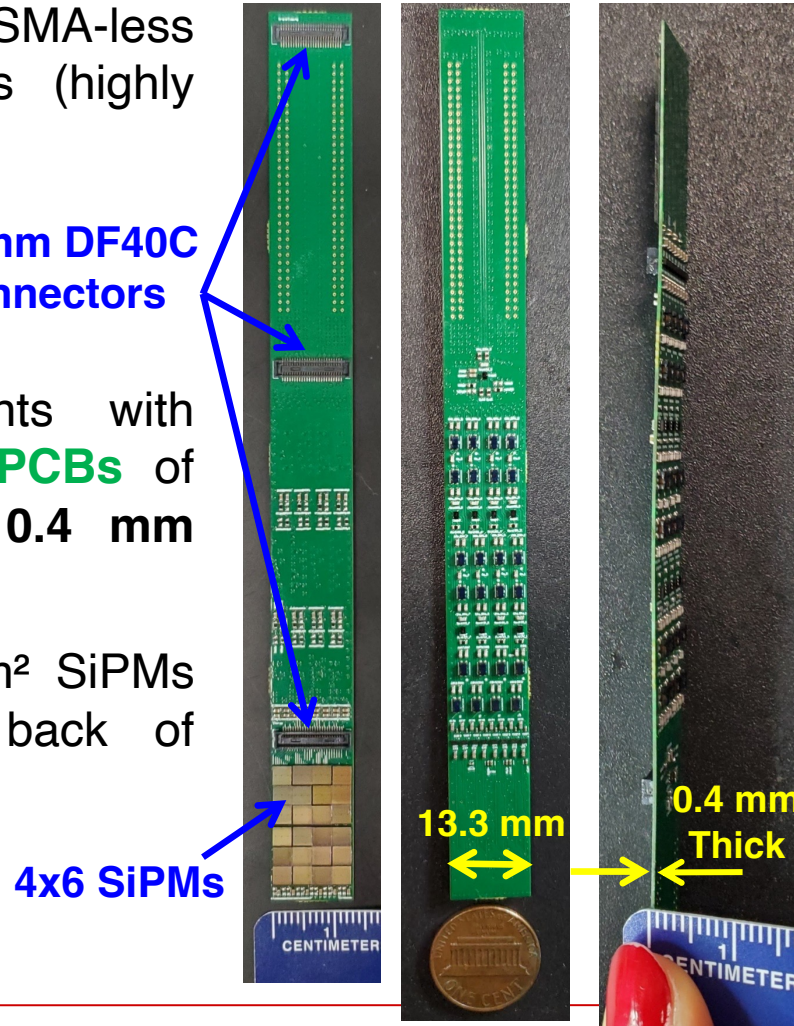
0.4 mm DF40C connectors

- **Timing** measurements with **green 4-layer FR4 PCBs** of **13.3 mm width** & **0.4 mm thickness**

- 4x6 array of 3x3 mm² SiPMs (photo-sensors) on back of **green timing board**

Bottom View

Top View



MIPS

Molecular Imaging
Program at Stanford

Stanford University

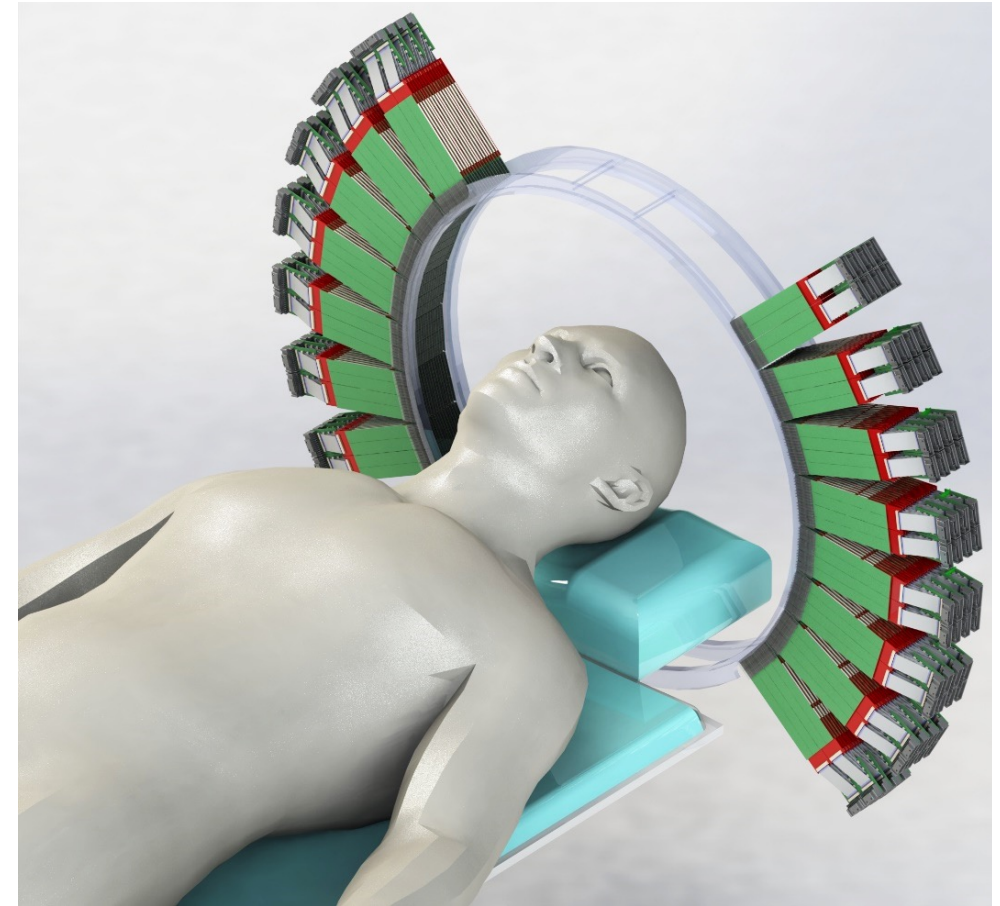
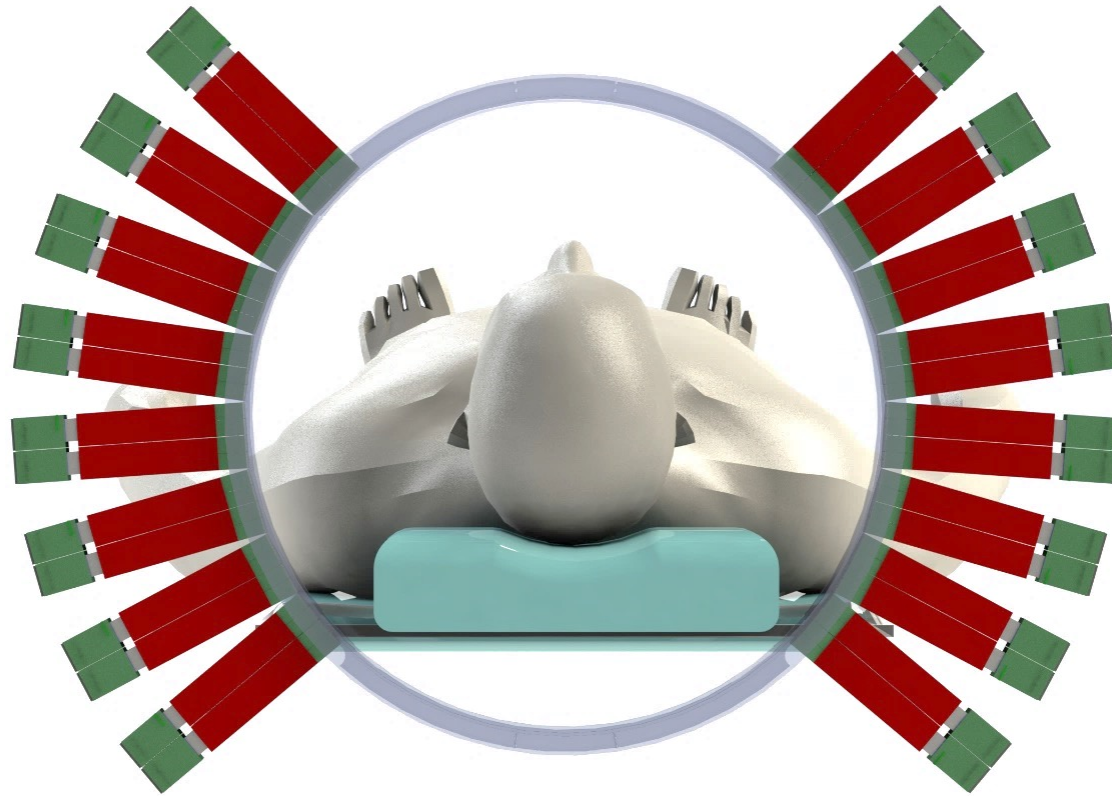
School of Medicine
Department of Radiology



Getting Closer to Final Goal: Partial-Ring TOF-PET (16 Detector Modules)



Stanford Cancer Imaging
Training Program



MIPS

Molecular Imaging
Program at Stanford

Stanford University

School of Medicine
Department of Radiology



Thank You!

and

Mentors:

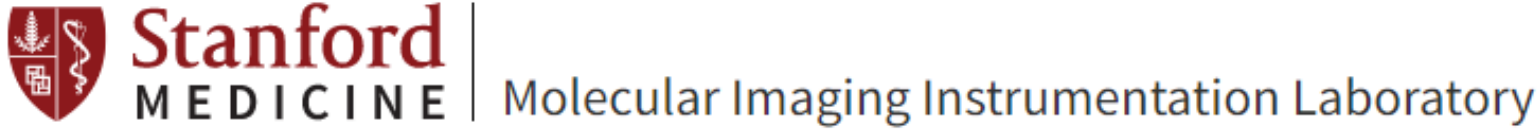
Drs. Andrei Iagaru & Craig Levin



Stanford Cancer Imaging
Training Program



(NIH T32 CA009695)



Marubeni
America Corporation



Xilinx University
Program



National Institutes
of Health

NIH research grants:

5R01CA21466903

&

1R01EB02512501



MIPS

**Molecular Imaging
Program at Stanford**

Stanford University

**School of Medicine
Department of Radiology**

